# Paper #: **12926-93 Vertebral Segmentation without Training** using Differentiable Appearance Modeling of a Deformable Spine Template

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Differentiable

in computer vision

Finds optimal scene

rendering process

optimization: simple,

powerful, and extensible

Gradient-based

parameters based on the

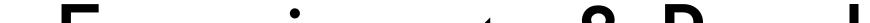
rendering [1]

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SPIE.

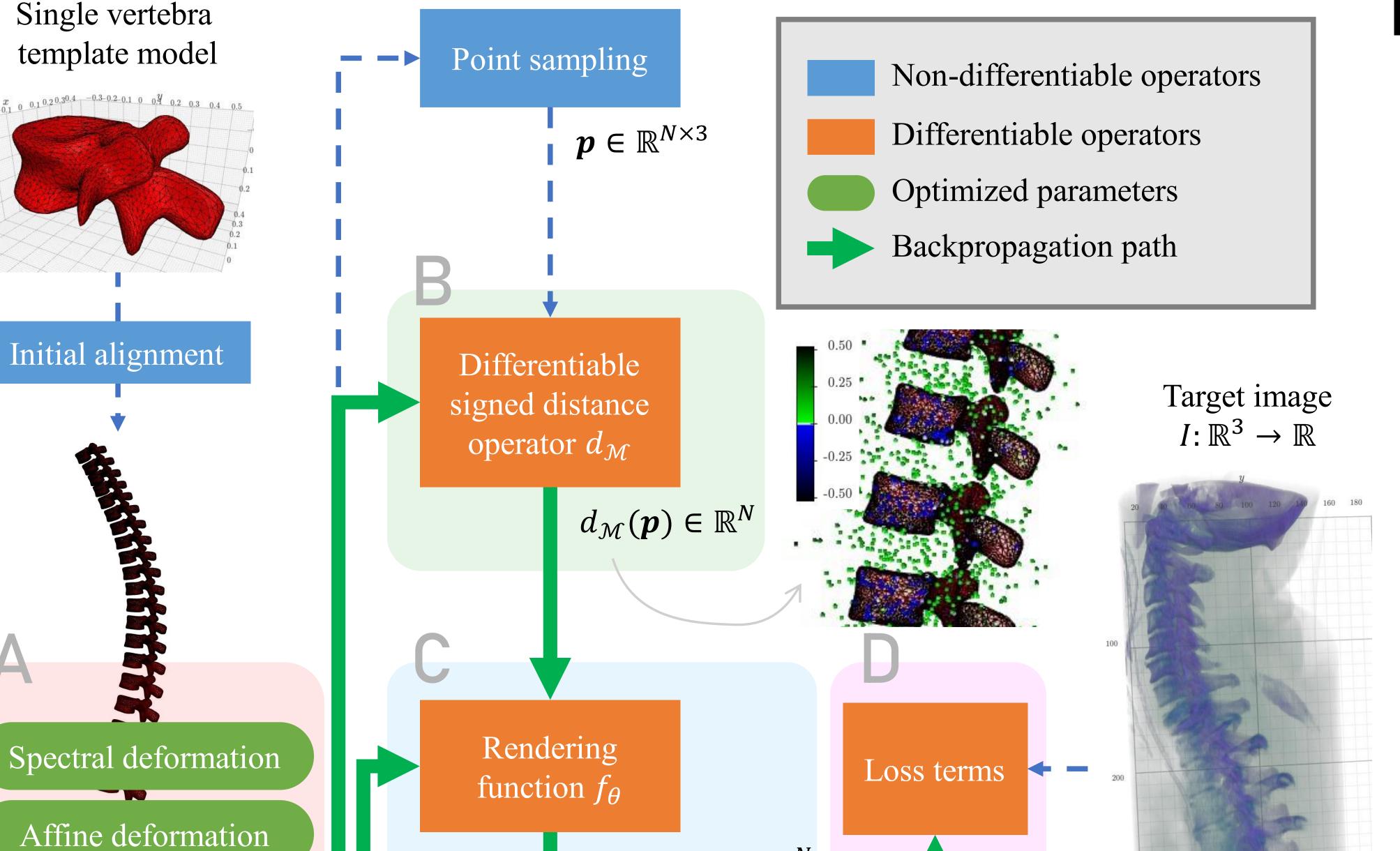
Given a spine template as the only prior knowledge, we perform vertebral segmentation by optimizing the shape and appearance through simple gradient descent, enabled by our novel differentiable template-to-image pipeline



## Introduction

Deformable model-based medical image analysis

- Provides correspondence information
- More transparent on reasoning Can work with significantly smaller dataset
- Our approach
- Differentiable Appearance Modeling
- Jointly optimizes the shape and appearance of the spine model to match the given CT image
- No training dataset required: Learning appearance only from the given image
- Why spine? High contrast surface + repetitive



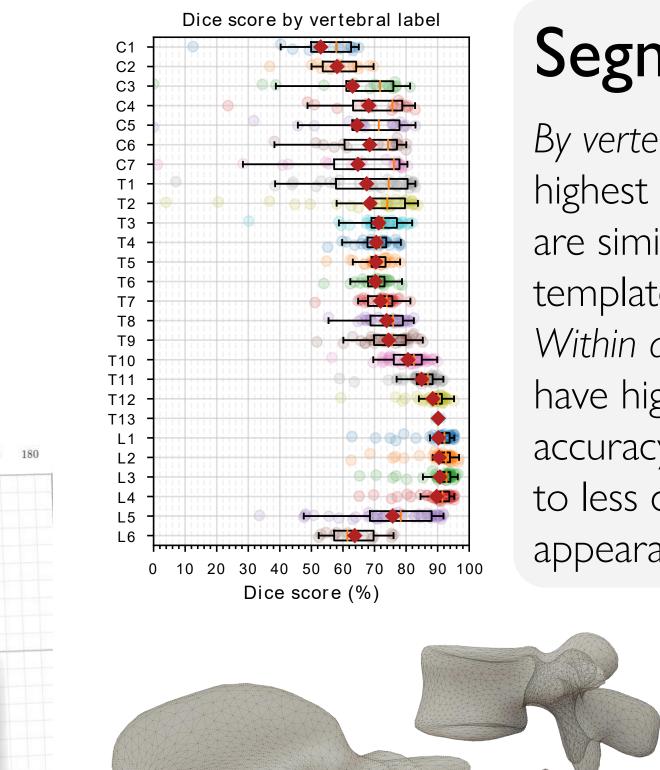
 $f_{\theta} \circ d_{\mathcal{M}}(\boldsymbol{p}) \in \mathbb{R}^{N}$ 

 $\uparrow$  Overview of our vertebral segmentation framework

### Experiments & Results

Our pipeline is tested on VerSe20' dataset [2] Vertebra template model is made from the average shape of xVertSeg lumbars [3]

KAIS



#### Segmentation

By vertebral label, lumbars have highest accuracy as their shapes are similar to lumbar-based template model. Within a vertebra, vertebral bodies have higher correspondence accuracy than vertebral arches due to less complex shape & varying appearance.

structures are easily exploitable to achieve the segmentation without large dataset

## Method

optimization  $\mathcal{M} \begin{pmatrix} A_i \in \mathbb{R}^{3 \times 3} \\ U_i \in \mathbb{R}^{V \times 3} \end{pmatrix}$ Spine model  ${\mathcal M}$  is described by affine deformation  $A_i$ and spectral coefficients  $U_i$ → Shape parameters with natural coarse-to-fine hierarchy  $U_i \leftarrow U_i - lr \times \left(\frac{\Lambda}{\lambda_0}\right)^{-\alpha} \times \frac{\partial \mathcal{L}}{\partial U_i}$ 

Spectral mesh

Differentiable signed distance operator  $d_{\mathcal{M}}: \mathbb{R}^3 \to \mathbb{R}$ The operator takes point positions and gives the signed distance from the surface mesh  ${\mathcal M}$  $\rightarrow$  Bridging shape & appearance  $\partial d_{\mathcal{M}}$  $\partial v_k$ Our backward step is allowing losses to propagate to the shape, accelerated by GPU + spatial structure

Spine model  $\mathcal{M}$ 

Appearance modeling  $f_{\theta} \colon \mathbb{R} \to \mathbb{R}$ Rendering function takes the signed distance and gives the appearance (voxel intensity) → Appearance model that fits high-contrast surfaces

Learnable function  $f_{\theta}$  is

Losses & optimization  $\mathcal{L}_{I}$  - Image similarity loss Guide appearance to match the given image (L1 loss)  $\mathcal{L}_{E}$  - Edge length regularizer Regulate mesh complexity  $\mathcal{L}_N$  - Normal regularizer

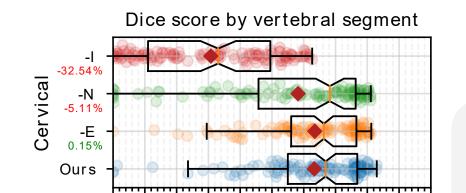
Align surface normal to image gradient  $\mathcal{L}_{O}$  - Overlap regularizer Penalize overlaps between meshes

 $\mathcal{L}_{V}$  - Variance regularizer Regulate shape variance between neighboring vertebra

Point sampling

 $\uparrow$  Vertebra template model used for the segmentation task

Correspondence error within a vertebra, selected from each segment (Top: cervical, Middle: thoracic, Bottom: lumbar)  $\rightarrow$ 



### Ablation study

 $\mathcal{L}_{I}$  is crucial for our optimization framework  $\mathcal{L}_N$  resolves ambiguous zeroisosurface for the rendering function  $\mathcal{L}_{E}$  improves the mesh quality,

rather than segmentation accuracy

# Conclusion

Dice score (%)

ອງ 10.50%

Differentiable Appearance Modeling allows robust and dataset-free analysis and easily adaptable to various neural network

Gradient is rescaled proportional to the eigenvalues Large  $\alpha \rightarrow$  coarse optimization Small  $\alpha \rightarrow$  fine control

modeled using a shallow neural network (Fourier feature transform + 3-layer MLP)

Increase sampling rate around the mesh surface AdamVector optimizer Reduce artifacts with vector-wise normalization Coarse-to-fine optimization Start optimization with low-passed image, gradually introduce high-freq. features

training/applications by being differentiable

Future works include developing holistic template models/sophisticated rendering functions and applying to image synthesis tasks

## References

[1] Kato, H. et al., "Differentiable rendering: A survey," arXiv preprint arXiv:2006.12057 (2020). [2] Sekuboyina, A. et al., "Verse: a vertebrae labelling and segmentation benchmark for multi-detector ct images," Medical image analysis 73, 102166 (2021). [3] Korez, R. et al., "A framework for automated spine and vertebrae interpolation-based detection and model-based segmentation," IEEE transactions on medical imaging 34(8), 1649–1662 (2015).

